

Excitation–contraction coupling in skeletal muscle of a mouse lacking the dihydropyridine receptor subunit $\gamma 1$

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1. In skeletal muscle, dihydropyridine (DHP) receptors control both Ca^{2+} entry (L-type current) and internal Ca^{2+} release in a voltage-dependent manner. Here we investigated the question of whether elimination of the skeletal muscle-specific DHP receptor subunit $\gamma 1$ affects excitation–contraction (E–C) coupling. We studied intracellular Ca^{2+} release and force production in muscle preparations of a mouse deficient in the $\gamma 1$ subunit ($\gamma -/-$).
2. The rate of internal Ca^{2+} release at large depolarization (+20 mV) was determined in voltage-clamped primary-cultured myotubes derived from satellite cells of adult mice by analysing fura-2 fluorescence signals and estimating the concentration of free and bound Ca^{2+} . On average, $\gamma -/-$ cells showed an increase in release of about one-third of the control value and no alterations in the time course.
3. Voltage of half-maximal activation ($V_{1/2}$) and voltage sensitivity (k) were not significantly different in $\gamma -/-$ myotubes, either for internal Ca^{2+} release activation or for the simultaneously measured L-type Ca^{2+} conductance. The same was true for maximal Ca^{2+} inward current and conductance.
4. Contractions evoked by electrical stimuli were recorded in isolated extensor digitorum longus (EDL; fast, glycolytic) and soleus (slow, oxidative) muscles under normal conditions and during fatigue induced by repetitive tetanic stimulation. Neither time course nor amplitudes of twitches and tetani nor force–frequency relations showed significant alterations in the $\gamma 1$ -deficient muscles.
5. In conclusion, the overall results show that the $\gamma 1$ subunit is not essential for voltage-controlled Ca^{2+} release and force production.

The transverse tubules of skeletal muscle cells contain a high density of DHP binding sites (reviewed by Lamb, 1992). Two functions have been assigned to the DHP-binding proteins (DHP receptors): the activation of a Ca^{2+} conductance (L-type Ca^{2+} current) with exceptionally slow kinetics, and the activation of intracellular release of Ca^{2+} from the sarcoplasmic reticulum (SR) (reviewed in Melzer *et al.* 1995). The latter process is probably the result of direct interaction between DHP receptor and Ca^{2+} -release channels (ryanodine receptors) (reviewed in Melzer & Dietze, 2001) and does not depend on Ca^{2+} entering the cell during the depolarization (Spiecker *et al.* 1979; Brum *et al.* 1988; Dirksen & Beam, 1999). The transverse tubular DHP receptor forms a heteropentameric complex consisting of the voltage-sensitive, channel-forming polypeptide α_{1S} that contains the DHP binding sites and molecular determinants for interaction with the ryanodine receptor (Grabner *et al.* 1999) and four auxiliary subunits: β , γ , α_2 and δ (for review see Walker

& De Waard, 1998). α_{1S} and β have been shown to be essential for E–C coupling (Beam *et al.* 1986; Gregg *et al.* 1996) and their elimination is lethal. The fact that the γ subunit ($\gamma 1$ isoform) could only be detected in skeletal muscle also suggests a role for this polypeptide that is important for muscle function (Jay *et al.* 1990; Powers *et al.* 1993; Wissenbach *et al.* 1998). $\gamma 1$ is a transmembrane protein of 32 kDa (222 amino acid residues) containing four putative membrane-spanning segments (Bosse *et al.* 1990; Jay *et al.* 1990). Functional studies of the $\gamma 1$ subunit have up to now been restricted to measuring transmembrane ionic currents. The effects of $\gamma 1$ on Ca^{2+} or Ba^{2+} inward currents have been investigated by coexpression of the subunit with the cardiac muscle α_{1C} subunit in heterologous expression systems (Singer *et al.* 1991; Wei *et al.* 1991; Lerche *et al.* 1996; Eberst *et al.* 1997; Sipos *et al.* 2000). An alternative approach to studying the role of subunits is the use of specific knockout systems. A recently generated $\gamma 1$ -deficient

mouse now permits the study of the effects of $\gamma 1$ on α_{1S} in its normal environment (Freise *et al.* 2000). In myotubes of neonatal $\gamma 1$ -deficient mice, a change in the voltage dependence of slow inactivation and enhanced activation of inward current have been reported (Freise *et al.* 2000). Because of the skeletal muscle specificity of $\gamma 1$ and because of the critical role of the DHP receptor in controlling Ca^{2+} release in skeletal muscle, one might expect $\gamma 1$ to play a crucial part in this process. Attempts have been made, but they failed to reconstitute voltage-controlled Ca^{2+} release by coexpressing ryanodine receptors and DHP receptor subunits in non-muscle cells (Takekura *et al.* 1995). Here we describe the first investigation of E–C coupling in $\gamma 1$ -deficient mice. We focused on the voltage-dependent activation process. For this purpose we studied the time course of activation of Ca^{2+} release in primary cultured myotubes and its voltage dependence as well as characteristics of contraction of mature fast and slow muscles under both normal and fatigue conditions.

METHODS

Experimental animals

$\gamma +/+$ and $\gamma -/-$ mice carrying the 129SVJ genetic background were used for the experiments. They were bred and kept in the essential specific pathogen-free animal facility of the University at Homburg. The procedure of generating the $\gamma -/-$ mouse has been described by Freise *et al.* (2000). We used mice ranging in age from 78 to 150 days for $\gamma +/+$ and from 58 to 141 days for $\gamma -/-$. The animals were killed by exposure to a rising concentration of CO_2 , in agreement with the regulations of the local animal welfare committee. The genotype of the mice was confirmed by a polymerase chain reaction assay using tail clips.

Cell culture

Pieces of muscle weighing 100–400 mg were excised from the hindlimbs, cut into small pieces and subjected to enzymatic dissociation at 37 °C for 60 min. The dissociation solution consisted of F12 medium (Gibco) and contained 1.5 mg ml⁻¹ collagenase (17449, Serva I), 2 mg ml⁻¹ protease (P6141, Sigma Type IX), 50 µg ml⁻¹ gentamycin (Biochrom), 2 mM Hepes, pH 7.2. After filtering (pore size 20 µm), the suspension was centrifuged and the pellet was resuspended in F12/CMRL growth medium with 5% fetal calf serum (Gibco) and 5% horse serum (Gibco) and seeded in culture flasks. Two days later the cells were detached from the flasks by trypsin solution (0.15% trypsin and 0.08% EDTA in Ca^{2+} - and Mg^{2+} -free phosphate-buffered saline (PBS)) and plated on carbon- and collagen-coated coverslips. The next day the medium was changed to F12/CMRL medium with 5% horse serum to induce differentiation. Throughout the culture, the cells were kept at 37 °C. Most measurements were carried out 4–7 days after reduction of the serum concentration.

Experimental solutions

The solutions for fluorescence and current measurements had the following composition. Bathing solution (mM): 130 tetraethylammonium hydroxide (TEA-OH), 127 HCl, 10 CaCl_2 , 1 MgCl_2 , 10 Hepes, 2.5 4-aminopyridine (4-AP), 0.0013 tetrodotoxin (TTX); pH was adjusted with HCl to 7.4. Pipette solution (mM): 145 CsOH, 110 HCl, 1.5 CaCl_2 (resulting in 20 nM free Ca^{2+}), 10 Hepes, 15 EGTA, 5 MgATP, 5 sodium creatine phosphate, 0.2 fura-2 (pentapotassium salt), pH 7.2. The Krebs–Ringer solution used for contraction measurements (purchased from Gibco) was composed of (mM): 118

NaCl, 3.4 KCl, 0.8 MgSO_4 , 1.2 KH_2PO_4 , 11.1 glucose, 25.0 NaHCO_3 , 2.5 CaCl_2 , pH 7.4.

Current measurements and analysis

Myotubes were voltage clamped in the whole-cell configuration with an EPC-7 patch-clamp amplifier with an extended range of capacitance compensation (1000 pF). Pipettes were pulled from borosilicate glass and had resistances between 1.5 and 2 MΩ when filled with pipette solution. Fluorescence and current data were recorded simultaneously at 4 kHz using a DA/AD interface (Digidata 1200, Axon Instruments) connected to a 486DX computer. For data acquisition and analysis the pCLAMP 6.0 software package (Axon Instruments) and Excel (Microsoft) were used. The last 8 ms of depolarization in each trace were averaged and plotted *vs.* voltage. To obtain the current–voltage relations of the L-type current, the data were least-squares fitted with eqn (1) in which the first term is used to correct for a linear leak component:

$$I(V) = g_{\text{leak}}(V - V_{\text{leak}}) + f(V)g_{\text{Ca,max}}(V - V_{\text{Ca}}), \quad (1)$$

$$f(V) = 1/\{1 + \exp((V_{1/2} - V)/k)\}. \quad (2)$$

Here, g_{leak} and V_{leak} are the conductance and reversal potential of the leak component and $g_{\text{Ca,max}}$ and V_{Ca} are the maximal conductance and reversal potential of the Ca^{2+} current. The gating function $f(V)$ is defined by eqn (2). $V_{1/2}$ and k are the voltage of half-maximal activation and the voltage sensitivity, respectively.

Fluorescence measurements and determination of Ca^{2+} release

The cells were loaded with the indicator dye (see above) by diffusion from the patch pipette. Fura-2 fluorescence was detected with a photomultiplier system (SF, Zeiss) attached to an inverted epifluorescence microscope (IMT-2, Olympus) at the emission wavelength of 510 nm (interference filter: Omega Optical, bandwidth 40 nm). Excitation wavelengths of 380 nm (for Ca^{2+} signals) and 358 nm (isosbestic point) were used (interference filters: Schott, bandwidth 14 and 9 nm, respectively). The experiments were carried out at room temperature (20–23 °C).

Using the ratio of the fluorescence signals (F_{380}/F_{358}) at the two excitation wavelengths, free Ca^{2+} and Ca^{2+} input flux, i.e. the total flux of Ca^{2+} into the myoplasm, were estimated as described by Dietze *et al.* (2000). The Ca^{2+} flux was calculated using a program written in Delphi (Borland International, Scotts Valley, CA, USA) (for equations see Baylor *et al.* 1983, and Brum *et al.* 1988) assuming the presence of fura-2 (0.2 mM), EGTA (15 mM) and troponin C (0.24 mM of fast Ca^{2+} -specific T-sites and 0.24 mM of slow Ca^{2+} - Mg^{2+} sites with parvalbumin-type behaviour, P-sites; rate constants from Baylor & Hollingworth, 1998) as intracellular Ca^{2+} buffers. The binding parameter values used were as follows. Fura-2: $k_{\text{on,Ca,Fura}} = 173 \mu\text{M}^{-1} \text{s}^{-1}$, $k_{\text{off,Ca,Fura}} = 30 \text{s}^{-1}$ (Dietze *et al.* 1998); T-sites: $k_{\text{on,Ca,T}} = 88.5 \mu\text{M}^{-1} \text{s}^{-1}$, $k_{\text{off,Ca,T}} = 115 \text{s}^{-1}$; P-sites: $k_{\text{on,Ca,P}} = 41.7 \mu\text{M}^{-1} \text{s}^{-1}$, $k_{\text{off,Ca,P}} = 0.5 \text{s}^{-1}$, $k_{\text{on,Mg,P}} = 0.033 \mu\text{M}^{-1} \text{s}^{-1}$, $k_{\text{off,Mg,P}} = 3 \text{s}^{-1}$. For EGTA we chose the rate constants of Smith *et al.* (1984): $k_{\text{on,Ca,EGTA}} = 1.5 \mu\text{M}^{-1} \text{s}^{-1}$, $k_{\text{off,Ca,EGTA}} = 0.3 \text{s}^{-1}$ and a modified set (same K_D) to obtain close to zero release immediately after repolarization (see Results and Dietze *et al.* 2000). $\Delta F/F$, the depolarization-induced fluorescence change divided by the resting fluorescence at the same wavelength, was used for determining the voltage dependence of the release process.

Contraction measurements

Both EDL and soleus muscles were dissected from the hindlimbs of the animals and mounted vertically in an organ bath filled with Krebs–Ringer solution (see Solutions) that was saturated with carbogen (95% O_2 –5% CO_2) by continuous bubbling and held at a temperature of 25 °C. The muscles were stretched to optimal length and stimulated via platinum field electrodes using 1 ms

supramaximal shocks (20 V). Isometric force was measured with a force-voltage transducer (Model FT03, Grass Instruments, Quincy, USA). The force signals were digitized with a Digidata 1200 analog-digital board (Axon Instruments). The sampling frequency was 1 kHz. Data sampling was synchronized with the output of TTL pulses that triggered the analog device used for extracellular stimulation. Data acquisition and analysis were carried out by software written in Delphi (Borland) running on a Pentium computer.

Statistics

Mean data are presented and plotted as means \pm S.E.M. (n = number of experiments). Student's two-sided t test was used to test for significant differences of mean values (assuming two independent populations; $P=0.05$ unless otherwise stated). Statistical power calculations were carried out using software tools provided by R. V. Lenth on the public domain of the Department of Statistics and Actuarial Science, University of Iowa (www.stat.uiowa.edu/~rlenth/) and with the program Power and Precision (version 1.20, Biostat, Teaneck, NJ, USA).

RESULTS

Ca²⁺ release rate in myotubes

We chose primary cultured myotubes derived from satellite cells of adult muscle to compare Ca²⁺ release in $\gamma +/+$ and $\gamma -/-$ muscle under voltage-clamp conditions. Myotubes have been used in various molecular physiology studies as model systems to investigate voltage-controlled Ca²⁺ release of skeletal muscle and they show characteristics of this process similar to mature vertebrate muscle (e.g. Garcia & Beam, 1994; Strube *et al.* 1996; Dietze *et al.* 1998, 2000).

Satellite cells were enzymatically isolated from the mouse skeletal muscle tissue and cultured as described in Methods. After seal formation and breaking the patch, the loading of the myotube with the artificial internal solution of the pipette was observed by the rise of the fura-2 resting fluorescence. After at least 5 min loading time, stimulation of internal Ca²⁺ release was started by applying depolarizing pulses of 100 ms duration from the holding potential of -90 mV.

We used the fluorescence decrease of fura-2 at 380 nm excitation that originates from Ca²⁺ release to estimate the rate of Ca²⁺ release as described previously (Dietze *et al.* 1998, 2000). The procedure is shown in Fig. 1 for a single depolarization to $+20$ mV in a $\gamma +/+$ (Fig. 1A) and a $\gamma -/-$ (Fig. 1B) myotube, respectively. It first involves the calculation of free Ca²⁺ (b panels) from the fura-2 ratio signal (a panels; Klein *et al.* 1988) and in a second step the calculation of total myoplasmic Ca²⁺ by solving a set of differential equations describing the binding of Ca²⁺ to myoplasmic binding sites (Baylor *et al.* 1983). The time derivative of the total myoplasmic Ca²⁺ is the input flux of Ca²⁺ into the myoplasmic space (c panels). The method suffers from the fact that parameters such as the concentrations of intrinsic binding sites and their binding rate constants that are used in the calculation have to be assumed, based on biochemical data from other vertebrate muscles. To mitigate this problem, we applied a high concentration (15 mM) of the chelator EGTA together with the

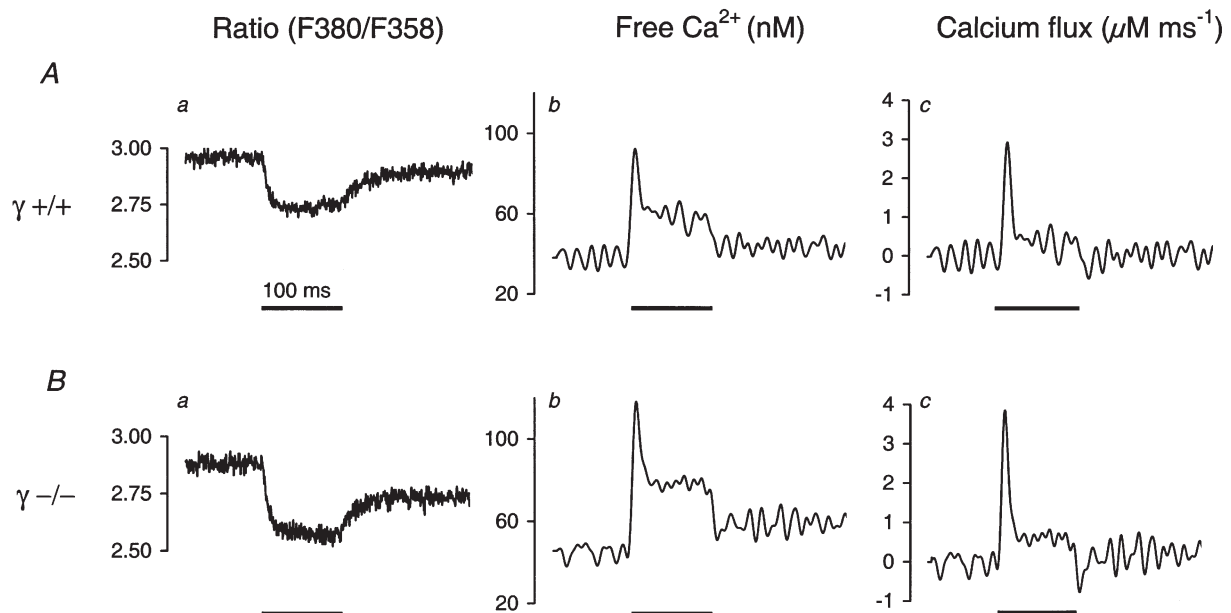


Figure 1. Estimating the time course of Ca²⁺ release in myotubes using fura-2 fluorescence transients

A, ratio F_{380}/F_{358} of single fura-2 fluorescence signals obtained at a 100 ms depolarization to $+20$ mV (horizontal bar) in a $\gamma +/+$ myotube (a), calculated free Ca²⁺ after correction for the indicator time response (b) and Ca²⁺ input flux (c) (see Results and Methods). B, corresponding calculations for a $\gamma -/-$ myotube.

indicator, a method that was originally introduced by Gonzalez & Rios (1993) for experiments on frog muscle fibres. Under these conditions EGTA dominates intracellular Ca^{2+} binding. Therefore, errors made in quantifying intrinsic binding sites and consequently possible differences in the expression of Ca^{2+} -binding proteins between the two groups of cells will be of minor effect (Dietze *et al.* 1998). In addition, the EGTA prevents movement artefacts and avoids excessive saturation of the indicator dye. In Fig. 1 we used the rate constants of EGTA determined by Smith *et al.* (1984) *in vitro* for the input Ca^{2+} flux estimate (see Methods).

Figure 2 shows averaged calculation results of signals obtained with pulses to +20 mV from 23 γ +/+ (A) and 14 γ -/- experiments (B). Similar to a previous study on porcine myotubes (Dietze *et al.* 2000), an undershoot of the calculated input flux below baseline values resulted (a

panels) when using the same set of literature values for the rate constants as in Fig. 1. This undershoot could be reduced by increasing the values of both EGTA rate constants. A minimal undershoot relative to the signal amplitude was obtained when raising both rate constants tenfold (b panels in Fig. 2). The overall shape of the flux time course changed relatively little. The thin lines indicate the standard errors of the means. The higher peak release rate of the γ -/- cells (32.6% increase in (a) and 32.0% in (b)) was statistically significant at $P=0.01$. Similarly, the total Ca^{2+} released within 100 ms of depolarization at +20 mV was about 30% higher in the γ -deficient cells (see legend of Fig. 2). These estimated alterations were independent of the choice of EGTA parameters. On the other hand, the ratio of the peak : end values of the rate of release was not significantly different (γ +/+: 6.18 ± 1.11 (Fig. 2Aa) and 4.08 ± 0.35 (Fig. 2Ab); γ -/-: 6.17 ± 0.52 (Fig. 2Ba) and 3.82 ± 0.23 (Fig. 2Bb)).

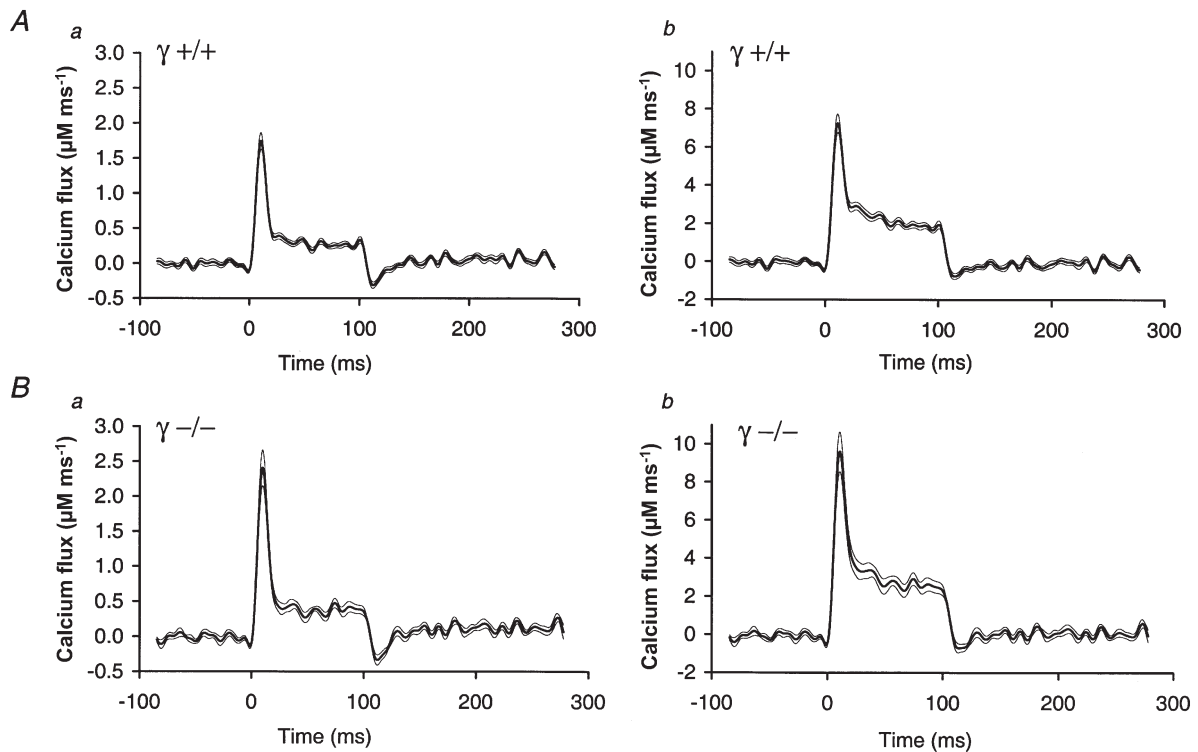


Figure 2. Mean time course of the Ca^{2+} release rate in myotubes

Comparison of calculated Ca^{2+} release rate using the means of 23 measurements in γ +/+ myotubes (A) and 14 measurements in γ -/- myotubes (B). Release was activated by a 100 ms depolarization to +20 mV. For panels Aa and Ba, the parameters used in the calculation were the same as in Fig. 1. In panels Ab and Bb, the rate constants of EGTA were altered at constant K_D to match more accurately the condition of zero release following repolarization to the holding potential. Thin lines indicate S.E.M. On average, the peak release rate in the γ -/- cells was about one-third higher than the value estimated for γ +/+: $2.41 \pm 0.26 \mu\text{M ms}^{-1}$ vs. $1.75 \pm 0.12 \mu\text{M ms}^{-1}$ in a and $9.60 \pm 1.00 \mu\text{M ms}^{-1}$ vs. $7.27 \pm 0.47 \mu\text{M ms}^{-1}$ in b. The release rate during the steady level (averaged over the last 10 ms of the pulse) was similarly different: $0.39 \pm 0.06 \mu\text{M ms}^{-1}$ vs. $0.25 \pm 0.03 \mu\text{M ms}^{-1}$ in a and $2.51 \pm 0.29 \mu\text{M ms}^{-1}$ vs. $1.78 \pm 0.12 \mu\text{M ms}^{-1}$ in b. These changes led to a corresponding fractional increase of the total Ca^{2+} released during the pulse (a, 31.2%; b, 29.7%). Free Ca^{2+} values immediately before the pulses derived from the resting fluorescence ratios were 49 ± 10 nM in γ +/+ and 72 ± 14 nM in γ -/-. They were not significantly different ($P=0.15$).

Voltage dependence of Ca^{2+} current and Ca^{2+} transients in myotubes

The calculation of free Ca^{2+} and of release involved numerical derivatives. To obtain a sufficient signal-noise ratio for the release estimates at smaller depolarizations requires signal averaging. Because the stability of the cells generally did not permit us to carry out the required number of measurements, the voltage dependence of the release process was determined by using the original fluorescence records at different voltage steps. Figure 3*A* and *B* exemplifies records of Ca^{2+} signals (*b* panels) and simultaneously measured Ca^{2+} inward currents (*a* panels) in individual myotubes of $\gamma +/+$ and $\gamma -/-$ animals, respectively.

The data for the current-voltage relations (*c* panels) and for the activation of conductance and Ca^{2+} release (*d*

panels) in Fig. 3 were obtained by averaging results from 14 $\gamma +/+$ (Fig. 3*A*) and 8 $\gamma -/-$ cells (Fig. 3*B*). The fitting procedures described in Methods were applied for each cell individually. From the raw current data, the fitted linear leak component was subtracted and eqn (1) was solved for the fractional conductance activation $f(V)$. The means of the fitted parameters of the different cells are listed in the figure legend and were used for constructing the continuous curves in Fig. 3*Ad* and *Bd*.

The activation characteristics of both groups of cells were similar to those reported by Dietze *et al.* (1998) for myotubes of the mouse diaphragm: the Ca^{2+} current had its threshold at about -20 mV and reached its maximum at about 12 mV. Ca^{2+} signals were activated at less depolarizing potentials. However, the voltage of half-maximal activation, $V_{1/2}$, and the voltage sensitivity

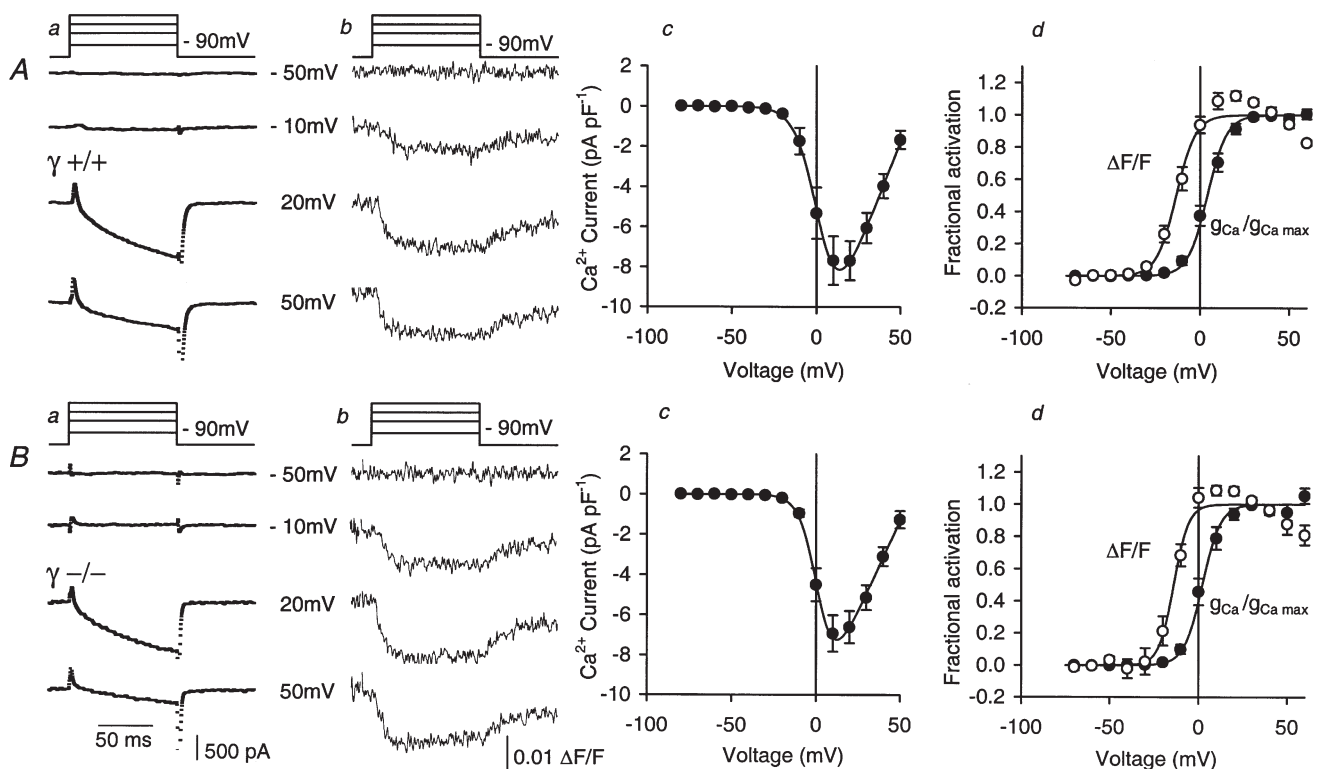


Figure 3. Voltage dependence of L-type Ca^{2+} conductance and Ca^{2+} release in myotubes

A, typical Ca^{2+} inward currents (*a*) and fluorescence transients ($\Delta F/F$) (*b*) at different voltages, mean current-voltage relation (*c*) and normalized activation curves (*d*) of Ca^{2+} conductance (●) and Ca^{2+} release (○) in 14 experiments on $\gamma +/+$ myotubes. Best-fit parameter values of individual fits by eqn (1) and (2): $g_{\text{Ca,max}} = 211 \pm 22$ pS pF $^{-1}$, $V_{\text{Ca}} = 59 \pm 2$ mV, $V_{1/2} = 4.11 \pm 1.84$ mV, $k = 5.44 \pm 0.26$ mV. Fluorescence: $V_{1/2} = -12.72 \pm 1.70$ mV, $k = 4.91 \pm 0.36$ mV. The curves were drawn using these parameter values. *B*, corresponding data to *A* of individual measurements (*a* and *b*) and mean values (*c* and *d*) of 8 experiments on $\gamma -/-$ myotubes. Best-fit parameters: $g_{\text{Ca,max}} = 180 \pm 21$ pS pF $^{-1}$, $V_{\text{Ca}} = 57 \pm 2$ mV, $V_{1/2} = 2.15 \pm 2.10$ mV, $k = 5.10 \pm 0.52$ mV. Fluorescence: $V_{1/2} = -13.56 \pm 2.91$ mV, $k = 4.04 \pm 0.53$ mV. Maximal inward current, maximal inward current density and voltage of maximal inward current were not significantly different: 1.06 ± 0.16 nA, 8.28 ± 1.18 pA pF $^{-1}$ and 14.3 ± 1.6 mV, respectively, in the $\gamma +/+$ group *vs.* 1.14 ± 0.20 nA, 7.00 ± 0.84 pA pF $^{-1}$ and 11.9 ± 2.0 mV, respectively, in the $\gamma -/-$ group. Similarly, cell capacitance, series resistance, g_{leak} and V_{leak} showed no significant difference: 133 ± 18 pF, 5.83 ± 0.43 M Ω , 17.32 ± 5.87 pS pF $^{-1}$ and 20.4 ± 4.1 mV, respectively, for $\gamma +/+$ *vs.* 149 ± 14 pF, 6.86 ± 1.23 M Ω , 17.65 ± 4.17 pS pF $^{-1}$ and 14.4 ± 2.81 mV, respectively, for $\gamma -/-$.

parameter k of both Ca^{2+} conductance and intracellular Ca^{2+} signal showed no significant difference between $\gamma^{-/-}$ and $\gamma^{+/+}$ cells (for values, see legend of Fig. 3). Similarly, the maximal current densities and maximal conductances were not significantly different. This was also the case for the set of experiments in Fig. 2 (current density at the end of the pulse: $10.42 \pm 0.77 \text{ pA pF}^{-1}$ in $\gamma^{+/+}$ vs. $8.92 \pm 1.06 \text{ pA pF}^{-1}$ in $\gamma^{-/-}$). The data, however, do not allow us to rule out a difference in the order of 20% of the maximal current density as reported by Freise *et al.* (2000) based on experiments on myotubes from neonatal mice.

In summary, the results described so far indicate only a modest increase in the Ca^{2+} release rate at large voltages in $\gamma^{-/-}$ myotubes.

Force activation in mature EDL and soleus muscle

To get information on E–C coupling of mature muscle we carried out experiments on isolated adult limb muscles

from the two groups of mice and measured contractions induced by extracellular electrical stimulation. To be able to distinguish between possible alterations specific to different types of muscle fibres, we chose the extensor digitorum longus (EDL) muscle, which consists primarily of fast twitch fibres, and the soleus muscle, which is a slow twitch muscle.

Figure 4A shows recordings of contractions obtained with single pulses and with repetitive stimulation. The frequency of stimulation varied between 25 and 150 Hz in EDL and between 10 and 100 Hz in soleus. In between the 350 ms stimulation intervals muscles were allowed to rest for 60 s.

To quantify contractile properties we measured peak tension, time to peak (t_{peak}) and half-time of relaxation ($t_{1/2}$) for single twitches, and maximal tension, time to half-maximal contraction within the 350 ms stimulation period ($t_{1/2, \text{contract}}$) and time to half-relaxation after the end

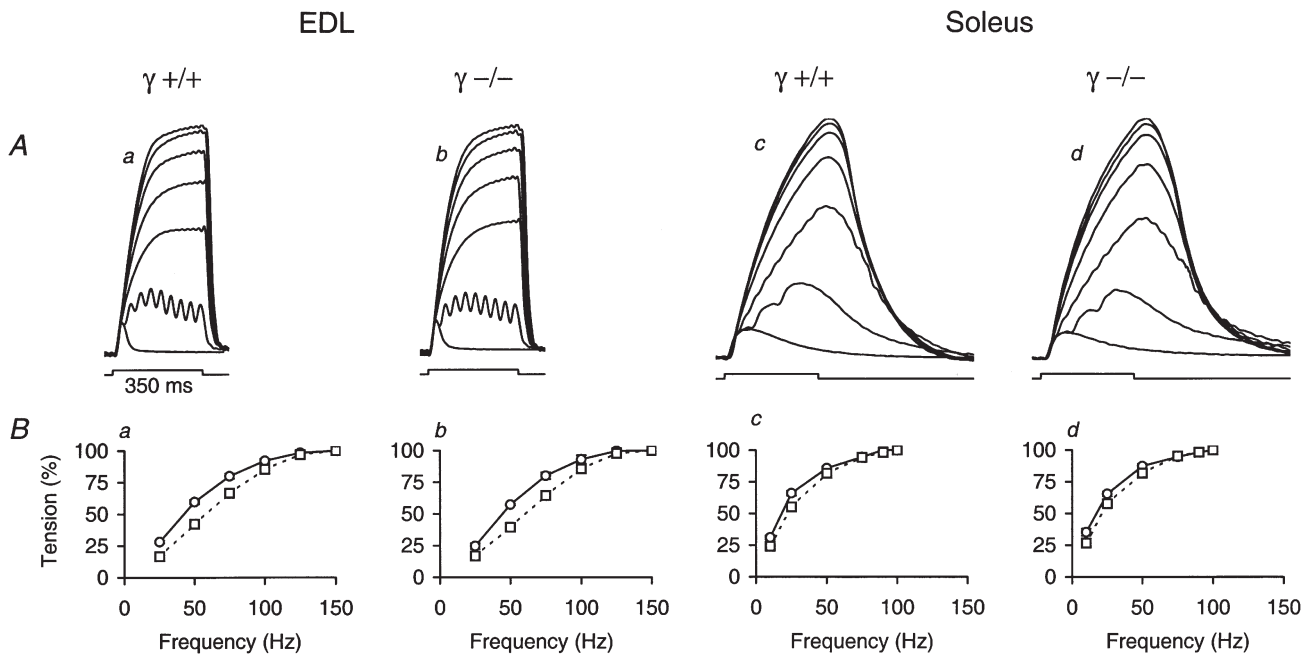


Figure 4. Contractile activation in fast and slow twitch muscles

A, single twitches and contractions measured at different stimulation frequencies in EDL (*a* and *b*) and soleus muscle (*c* and *d*). Example recordings of $\gamma^{+/+}$ (*a* and *c*) and $\gamma^{-/-}$ muscles (*b* and *d*) are shown. The rectangular signal below the traces shows the time interval of 350 ms in which repetitive stimulation was activated. Frequencies of 25, 50, 75, 100, 125 and 150 Hz were applied in EDL and of 10, 25, 50, 75, 90 and 100 Hz in soleus. The signals were normalized to the maximum. The maximal force values were 141 mN (*a*), 194 mN (*b*), 101 mN (*c*) and 74 mN (*d*). B, force–frequency relations derived from recordings similar to those shown in A. The normalized mean force values at the end of the stimulation period are plotted. In both $\gamma^{+/+}$ and $\gamma^{-/-}$, experiments were carried out on 4 EDL (*a* and *b*) and 3 soleus (*c* and *d*) muscles. The error bars indicating S.E.M. are smaller than the symbol sizes. \circ , measured before fatigue; \square , measured after stimulation leading to fatigue (tetanus amplitude 30% of original value in EDL and 50% in soleus, see Fig. 5) and a subsequent 30 min recovery interval. The mean values of the frequency that generated half-maximal force ($F_{1/2}$) were $42.47 \pm 1.01 \text{ Hz}$ ($\gamma^{+/+}$, $n = 4$) vs. $44.31 \pm 0.71 \text{ Hz}$ ($\gamma^{-/-}$, $n = 4$) for EDL and $18.17 \pm 0.73 \text{ Hz}$ ($\gamma^{+/+}$, $n = 3$) vs. $17.21 \pm 1.19 \text{ Hz}$ ($\gamma^{-/-}$, $n = 3$) for soleus. After fatigue and 30 min recovery the corresponding values were $57.90 \pm 1.89 \text{ Hz}$ ($\gamma^{+/+}$) vs. $60.29 \pm 2.08 \text{ Hz}$ ($\gamma^{-/-}$) for EDL and $22.50 \pm 0.79 \text{ Hz}$ ($\gamma^{+/+}$) vs. $21.39 \pm 1.79 \text{ Hz}$ ($\gamma^{-/-}$) for soleus.

	EDL ($n = 8$)				Soleus ($n = 7$)			
	$\gamma +/+$	S.E.M.	$\gamma -/-$	S.E.M.	$\gamma +/+$	S.E.M.	$\gamma -/-$	S.E.M.
Twitch								
Tension (mN)	23.27	1.46	20.38	2.34	8.98	0.70	8.48	0.53
t_{peak} (ms)	18.16	1.10	16.80	1.04	51.21	4.73	58.43	6.66
$t_{1/2}$ (ms)	26.13	1.43	24.63	1.85	98.83	22.85	121.38	32.66
Tetanus								
Tension (mN)	179.89	13.43	154.57	15.01	96.54	12.78	78.29	8.49
$t_{1/2,\text{contract}}$ (ms)	56.95	2.86	50.98	2.43	122.10	7.02	116.43	2.79
$t_{1/2,\text{relax}}$ (ms)	36.93	0.56	38.61	0.74	147.47	7.23	164.61	16.51
Twitch/tetanus	0.131	0.005	0.131	0.006	0.103	0.037	0.112	0.006

For each genotype, 8 experiments were carried out on EDL and 7 experiments on soleus muscle. For single twitches values are: peak tension; t_{peak} , time to peak; and $t_{1/2}$, half-time of relaxation. For tetani values are: maximal tension; $t_{1/2,\text{contract}}$, time to half-maximal contraction within the 350 ms stimulation period; and $t_{1/2,\text{relax}}$, time to half-relaxation after the end of stimulation.

of stimulation ($t_{1/2,\text{relax}}$) for tetani. The results are summarized in Table 1.

In addition, the force–frequency relation, i.e. the dependence of maximal force at the end of a fixed stimulation period (350 ms) on pulse frequency, was determined. Mean force–frequency relations measured before a fatigue procedure (see below) and following a 30 min recovery period after fatigue are shown in Fig. 4B. Alterations in the action potentials, in potentiation or inactivation of Ca^{2+} release or changes in the contraction time course, induced by preceding activation, will influence

the shape of this curve. The curves were defined by determining the frequency for half-maximal amplitude ($F_{1/2}$, see legend of Fig. 4 for values).

None of the contraction parameters of the $\gamma -/-$ muscles showed a statistically significant difference compared with $\gamma +/+$.

Fatigue in EDL and soleus muscle

A change in the function of $\gamma 1$ -deficient DHP receptors might reveal itself only under extreme physiological conditions. Notably, E–C coupling is one of the events

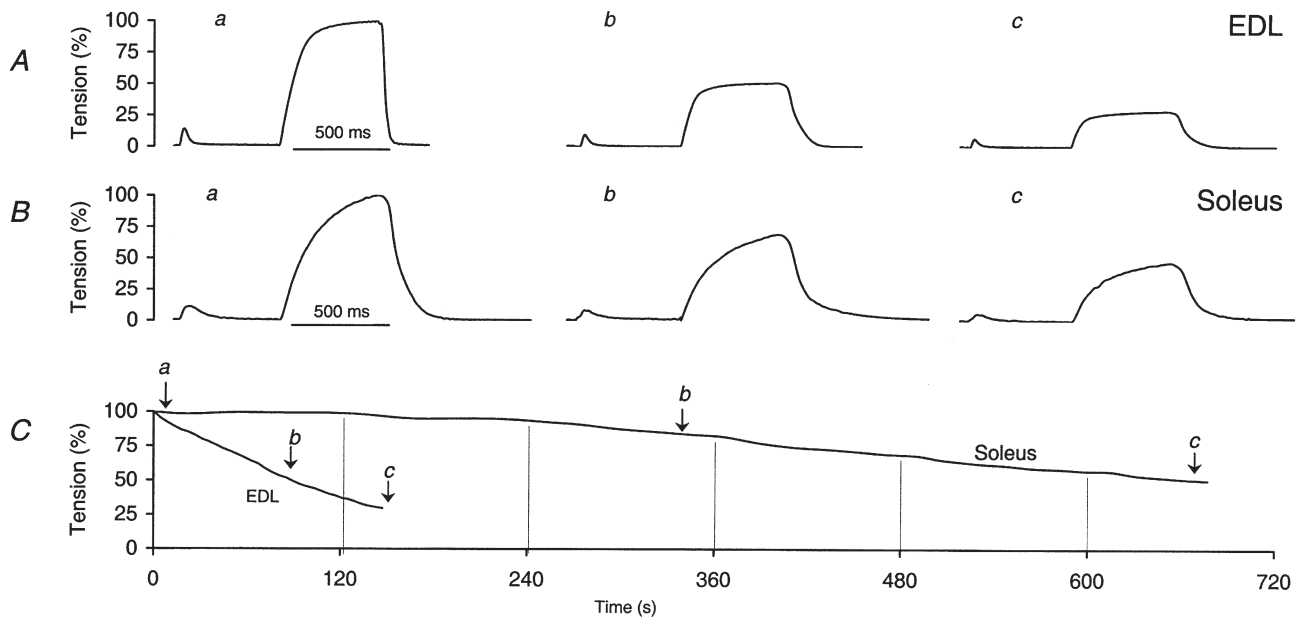


Figure 5. Fatigue in fast and slow twitch muscle

Examples of twitch and tetanus recordings in EDL (A) and soleus (B) at different times during fatigue stimulation (see text for details). C, amplitude change of tetanic contraction in EDL and soleus plotted against time to exemplify fatigue runs. a, b and c indicate the times when the signals shown in A and B were recorded. Vertical lines indicate times when the tetanus repetition rate was increased (see text for details).

Table 2. Comparison of twitch and tetanus parameters in fatigued γ +/+ and γ -/- muscles

	At T50%				At T30%							
	EDL (<i>n</i> = 4)		Soleus (<i>n</i> = 3)		EDL (<i>n</i> = 4)		Soleus (<i>n</i> = 3)					
	γ +/+	S.E.M.	γ -/-	S.E.M.	γ +/+	S.E.M.	γ -/-	S.E.M.				
Twitch												
Tension (mN)	18.27	1.35	15.64	1.22	5.58	1.32	8.47	0.59	13.44	1.07	10.73	0.93
t_{peak} (ms)	19.80	0.50	18.20	0.98	29.33	2.36	37.73	3.67	18.40	0.65	17.55	0.57
$t_{1/2}$ (ms)	25.10	1.97	25.20	2.56	65.46	8.08	91.33	1.93	25.30	1.98	24.70	2.30
Tetanus												
Tension (mN)	105.91	4.21	90.71	9.87	35.55	4.45	34.07	3.15	63.29	2.41	58.84	4.53
$t_{1/2, \text{contract}}$ (ms)	45.50	1.55	42.75	2.25	118.00	3.06	126.00	2.31	39.75	0.85	38.50	1.66
$t_{1/2, \text{relax}}$ (ms)	92.00	1.22	85.5	3.66	133.67	9.17	147.67	2.96	87.00	2.12	79.75	4.27
Twitch/tetanus	0.170	0.008	0.168	0.007	0.133	0.041	0.165	0.047	0.195	0.015	0.189	0.012

For each genotype four experiments were carried out on EDL and three experiments on soleus muscle. Values were determined when the tetanus amplitude had declined to 50% of its initial value (T50%) in EDL and soleus and to 30% in EDL (T30%). For definitions see Table 1 and for description see text.

that appear to be affected in muscle fatigue (for a review see Stephenson *et al.* 1998). Therefore, we carried out a series of experiments to study contraction of isolated fast and slow twitch muscles during periods of repetitive tetanic stimulation that lead to fatigue. A protocol similar to the one previously applied to single mouse muscle fibres by Lännergren & Westerblad (1991) was applied. Stimulation intervals (pulse frequency 125 Hz for EDL and 75 Hz for soleus) were initially separated by recovery intervals of 4 s. The duration of the recovery intervals was shortened by 20% every 2 min. The stimulation continued until a time when tetanic tension was reduced to 30% (T30%) and 50% (T50%) of the initial tension for EDL and soleus, respectively. A single twitch was applied 500 ms before each tetanus to determine twitch/tetanus ratios (Fig. 5*A* and *B*).

Figure 5 exemplifies the changes in amplitude and time course of twitches and tetani during a fatigue run for one EDL and one soleus experiment. Due to its higher oxidative capacity (Westerblad *et al.* 1991), soleus is considerably more resistant to fatigue than EDL. Note also the prolongation of relaxation in parallel with the progressive amplitude decrease in EDL.

To compare the changes of the tetanus parameters during fatigue in γ +/+ and γ -/- muscle for each genotype, four experiments were carried out on EDL and three experiments on soleus, respectively. The twitch/tetanus ratio increased slightly over time in EDL and remained essentially constant in soleus. The relaxation of the tetani in EDL became considerably slower within the first minute of stimulation and then the half-time of relaxation remained about constant at more than twice the initial value; there was no comparable change in soleus. Apart from a small increase in T30% of EDL ($P=0.048$), all differences between γ +/+ and γ -/- remained below the significance

threshold. Mean values of T30% (EDL) were 146.5 ± 2.3 s for γ +/+ and 166.8 ± 7.9 s for γ -/-. T50% values were 91.1 ± 2.2 s (γ +/) *vs.* 101.3 ± 4.3 s (γ -/-) in EDL and 655.0 ± 46.5 s (γ +/) *vs.* 732.5 ± 15.6 s (γ -/-) in soleus. The mean contraction parameters at T50% for EDL and soleus and at T30% for EDL are listed in Table 2.

It is known that after fatigue resulting from repeated tetanic stimulation the maximal tetanic force (i.e. obtained at high stimulation frequency) recovers more rapidly than the force obtained at low stimulation frequencies (Westerblad *et al.* 1993). In force–frequency relations this effect shows up as a shift to higher frequencies (Fig. 4*B*, dashed lines). The finding has been attributed to a depression of Ca^{2+} release (Westerblad *et al.* 1993) and might, therefore, be different in muscles with altered DHP receptors. However, the force–frequency relations obtained after fatigue were indistinguishable between controls and knockout muscle (Fig. 4*B*).

DISCUSSION

In an initial study on myotubes from neonatal mice deficient in the DHP receptor γ 1-subunit that focused on properties of the ionic current, it was reported that voltage-dependent inactivation became slower, that the voltage of half-maximal steady-state inactivation was displaced to depolarizing potentials and that the amplitude of inward current density increased, indicating enhanced Ca^{2+} influx during voltage-dependent activation (Freise *et al.* 2000).

In skeletal muscle the main source of Ca^{2+} for the activation of force is the sarcoplasmic reticulum. Voltage control of SR Ca^{2+} release is based on mechanical interaction between the DHP receptor and the ryanodine receptor ('conformational' E–C coupling, Rios *et al.* 1991). Because the tissue-specific expression of γ 1 suggested a skeletal muscle-specific function, it was suspected

(e.g. Wissenbach *et al.* 1998) that $\gamma 1$ may play a crucial role in E–C coupling. If this is the case, one should expect large effects of a specific knockout of the protein on physiological signals related to this process. Therefore, in this investigation we measured – in addition to Ca^{2+} inward currents – Ca^{2+} release and contraction in muscle of $\gamma 1$ -deficient mice.

While the Ca^{2+} inward flux can be determined directly by measuring the transmembrane current, the flux of Ca^{2+} release from the SR can only be estimated indirectly based on the measured indicator signals, and this estimate depends on assumptions made for the kinetics of Ca^{2+} binding to myoplasmic sites. We are aware of the fact that the determination is subject to a number of uncertainties. Nevertheless, the phasic–tonic time course of the Ca^{2+} input flux resembles the signals in adult amphibian and mammalian muscle fibres, similarly measured in the presence of millimolar intracellular EGTA (Shirokova *et al.* 1996). We, therefore, think that our determination comes close to the real time course. To search for differences in the release characteristics of two groups of cells, the approach used here definitely seems adequate.

The characteristics of depolarization-induced Ca^{2+} release, assessed at +20 mV in our myotubes derived from satellite cells of murine limb muscle, were similar to those described previously by our laboratory for myotubes from satellite cells of the mouse diaphragm or of the porcine longissimus dorsi muscle (Dietze *et al.* 1998, 2000). The rate of voltage-controlled Ca^{2+} release showed a maximum soon after the beginning of a depolarization and dropped to a lower non-zero level. Release remained under the control of membrane voltage during depolarizations lasting 100 ms because it could be lowered rapidly by repolarization to the holding potential (Fig. 2).

At the potential of +20 mV, peak and steady level rates of release in the $\gamma -/-$ cells were about one-third higher than in controls (see legend of Fig. 2). This result would be in line with the conclusion reached by Freise *et al.* (2000) that elimination of the $\gamma 1$ subunit may enhance rather than suppress the function of the DHP receptor. The observed difference in release rate at a potential leading to close to full activation may be due to a number of causes, for instance different efficiencies of coupling between DHP and ryanodine receptors or different degrees of loading of the SR. Our hypothesis that the gating characteristics might be altered and release might, therefore, show larger differences at other voltages could not be confirmed. Like the voltage dependence of activation of Ca^{2+} conductance, the voltage dependence of the Ca^{2+} signals showed no statistically significant change.

If the γ -subunit modulates SR Ca^{2+} release, its effect may be more pronounced in the native muscle tissue than in myotubes. In particular, the artificial solutions used for

the Ca^{2+} release determination are of concern. We, therefore, also investigated the force response of isolated adult limb muscles to single stimuli and repetitive stimulation. Here, muscle cells function under more physiological conditions. With the stimulation protocols used, which should cover most of the situations experienced by a muscle during normal activity, no alterations could be noticed in the $\gamma -/-$ muscles. The mean values of force amplitudes (Table 1) showed small decreases rather than increases (in contrast to the myotube results). The changes were, however, well below our threshold for statistical significance. In previous work, the persistent depression of the force response to low frequency stimulation after repetitive stimulation by short tetani ('low-frequency fatigue') has been shown to go along with smaller intracellular Ca^{2+} signals, indicating a suppression of Ca^{2+} release from the SR (Westerblad *et al.* 1993). This type of fatigue might therefore be affected by a structural alteration of the DHP receptor. However, the force–frequency relations after the repetitive tetanic stimulation (that revealed low-frequency fatigue – in particular in EDL) showed no difference between $\gamma +/+$ and $\gamma -/-$ muscle (Fig. 4B).

Thus, on the level of contractile activation of isolated skeletal muscle, there was no evidence for altered Ca^{2+} release as indicated by the myotube results. Yet we might make a type II error, i.e. accept the null hypothesis of no change despite the presence of changes that are hidden by the signal variances. Therefore, we estimated the probability of avoiding type II errors at different assumed effect sizes by calculating the 'statistical power' of the test (see Methods). We expect that the complete elimination of a crucial mechanistic element should produce a clear decrease or increase in functional parameters. At an assumed effect size of 50% change from the control value, almost all of the contraction data gave statistical power values above 0.8 (for 33 out of 42 investigated parameters we obtained values of 0.9 and higher) showing that a fractional change equal to or above 50% of the control is unlikely. Exceptions with very low power were the half-time of relaxation ($t_{1/2}$) of twitch in soleus (Table 1) and twitch force and twitch/tetanus ratio of soleus at T50%. At a power of 0.8, there was no increase in regular twitch force of larger than 20–30% in EDL and soleus. Therefore, it appears unlikely that in native muscle fibres the elimination of the $\gamma 1$ subunit causes a larger effect on peak Ca^{2+} release than the relatively small increase found in myotubes. Consequently our findings lead us to the conclusion that $\gamma 1$ plays no crucial role in skeletal muscle activation during E–C coupling. Smaller, more subtle changes, however, cannot be ruled out.

It seems surprising that the elimination of an accessory component exhibiting absolute specificity for a protein that proved to be essential for E–C coupling does not

have a more serious impact on this process. Recently, four putative isoforms with relatively low sequence identity to $\gamma 1$ have been described (Klugbauer *et al.* 2000). They are predominantly expressed in the brain, but one of these isoforms ($\gamma 5$) is also found in skeletal muscle. One might, therefore, argue that $\gamma 5$ could have replaced $\gamma 1$ in its function. However, heterologous expression using α_{1C} as the indicator subunit showed that $\gamma 5$ exerts none of the functional effects of $\gamma 1$ on the ionic current, suggesting that $\gamma 5$ does not interact with L-type channels. There is no evidence that $\gamma 5$ can be associated with the skeletal muscle DHP receptor, while all biochemical studies published so far show that $\gamma 1$ is a tightly associated component.

It is also possible that additional as yet unknown conditions must be met for a function of $\gamma 1$ on E–C coupling to become more evident. It is for instance known that certain point mutations in the α_{1S} subunit of the DHP receptor cause hypokalaemic periodic paralysis, a disease leading to sporadic muscle failure under conditions of hypokalaemia and an elevated concentration of insulin (reviewed in Lehmann-Horn & Jurkat-Rott, 1999). It may, therefore, be worthwhile to study the effect of other environmental factors, for instance hormonal activation of intracellular second messenger cascades, on the function of γ -deficient skeletal muscle in future experiments. Also, different protocols to enhance fatigue might be tried, perhaps using drugs interfering with ATP replenishment, because a slight increase in fatigue resistance of EDL may be indicated by the data (see legend of Table 2: T30% but not T50%). Furthermore, Ca^{2+} release at long depolarizations that lead to voltage-dependent inactivation may be altered in the γ -/- preparations. This process could be a strategic point in modulating the strength of Ca^{2+} release in skeletal muscle. Its investigation is experimentally challenging because in isolated muscle cells the Ca^{2+} release mechanism does not tolerate long depolarizations well. Nevertheless, such studies seem worthwhile because of the reported change of steady-state inactivation of L-type Ca^{2+} conductance (Freise *et al.* 2000).

In summary, elimination of the $\gamma 1$ subunit caused a mild increase of the voltage-activated Ca^{2+} release in myotubes from adult mice and no alteration in its voltage dependence. In mature muscle, contractile activation induced by a single excitation event or by short sequences of action potentials does not seem to be altered to any appreciable degree in the absence of $\gamma 1$ in either fast or slow twitch muscle. We conclude that the γ -subunit of the skeletal muscle DHP receptor plays no crucial part in the normal signal transduction leading from the sarcolemmal depolarization to SR Ca^{2+} release. Further studies are needed to decide whether $\gamma 1$ plays a modulatory role in skeletal muscle E–C coupling, perhaps leading to stronger functional changes under special conditions.

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